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The **Bionic** Human:

a talk by Christian Freudiger

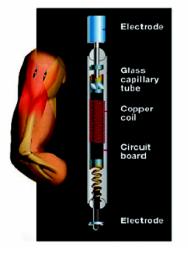


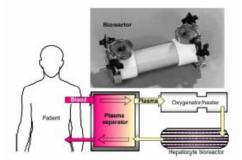
Overview

Implants and hybrid technologies find many fields of applications:

Artificial organs (e.g. liver)

Artificial muscles, bones and joints



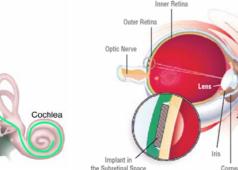




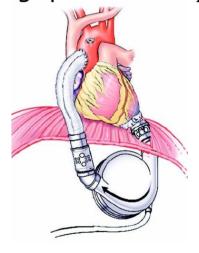
Sound

Transmitter

Receive



Circulatory support (e.g. pacemakers)





1. What's the problem

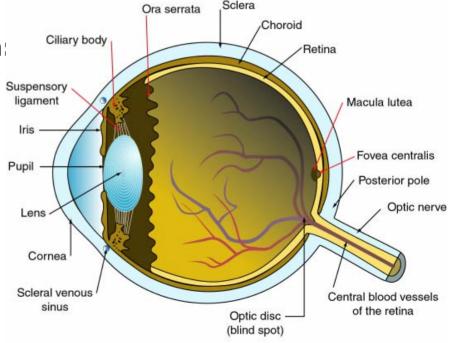
Features of the visual system:

- Resolution: 75 µm at distance of 25 cm (=angular difference of 1')
- refresh rate: approx. 40 Hz
- color contrast: approx. 100Mio different colors
- intensities: 60 Photons (=100W bulb in 600 km distance)

Functioning of the visual system:

1. Optical part:

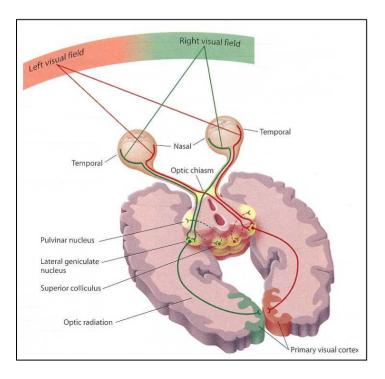
- reproduce sharp picture on the retina
- adjust light intensity

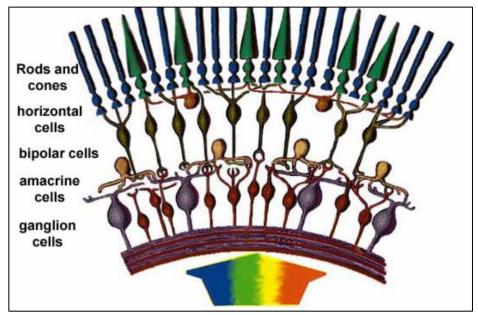




1. What's the problem

- 2. Detection (retina):
 - photoreaction with rhodopsin (1 photon)
- amplification cascade (x 10⁶)
 - ➔ action potential





3. Information processing (visual cortex)

- information form 130 Mio. photoreceptors
- reduction to 1.2 Mio specialized ganglion neurons
- enrichment with data from memory



1. What's the problem

Typical illnesses that could be healed:

- Retinitis Pigmentosa:
 - continuous degeneration of the retina
 - inherited blindness
 - most common form of blindness:
 1.5 million people affected worldwide
 (= 1 of 3500 births)
- Age-related macular degeneration:
 - continuous degeneration of rods in the macula (visual disk)
 - typical disease of older people
 - more and more people are affected
 70.000 new patients in the U.S. a year

But: neurons mainly stay alive







1. What's the problem

Different approaches to stimulate nerves of the visual system:

Cortical prosthesis:

direct stimulation of the visual cortex in the brain with electrodes:

- surface electrodes
- intracortical electrodes

First experiments in 1947 (wires through the skull)

Retinal prosthesis:

implant into the eye that replaces the retina (at least in parts)

Subretinal prosthesis:

replacement of photoreceptors by "solar cells"

Epiretinal prosthesis:

stimulation of ganglion cells with signal form external detector

Optic nerve prosthesis:

stimulation of the optical nerve (1.2 Mio ganglion cells within 2mmdiameter cylinder)

Method was mainly pursued in the 70s



1. What's the problem

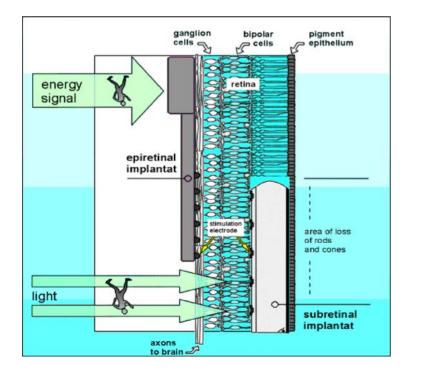
Types of retinal prosthesis

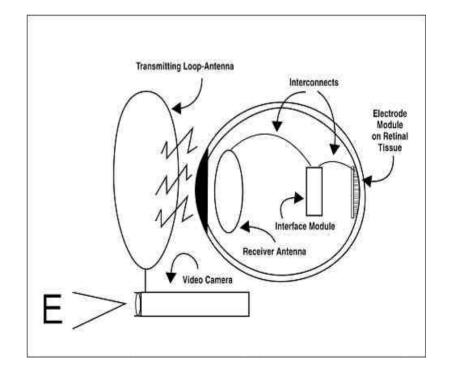
Subretinal prosthesis:

Replacement of photoreceptors in the retina by photosensitive devices

Epiretinal prosthesis

Stimulation of ganglion cells with signal form external detector (camera)







1. What's the problem

System-Engineering: Design of implant and fabrication Materials layout and encapsulation: system: - resistance

- protection of tissue

Understanding the nervous

- proper stimulation parameters
- suitable electrode design

How can physicists and engineers help?

Power supply and information transfer:

- inductive coupling
- converting near infrared light

Sensor design:

- photodiodes
- solar cells



Outline

Outline of the talk:

- 1. What's the problem
- 2. Functionality of neurons and consequences for stimulation
 - information transmission in neurons
 - electrical stimulation of neuronal activity
 - proper parameters and electrode design for effective stimulation
- 3. Sensor design: functionality of a solar cell and a photo-conductor
- 4. Wireless power supply and information transmission
- 5. Suitable materials and encapsulation
- 6. State of the art systems:
 - epiretinal prototypes
 - subretinal prototypes \rightarrow especialla MPDA

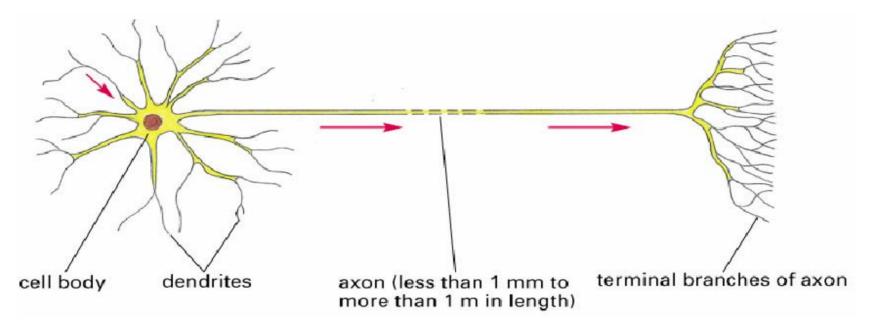
2. How does a human transmit information?

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2.1 How does the hand know, what the leg is doing?

The neuron (= nerve cell):



Difference between a "telephone cable" and a neuron:

- neurons are purely isolated
- bathed in a conductive bath

How can a leaky cable carry a sharp signal over a long distance?



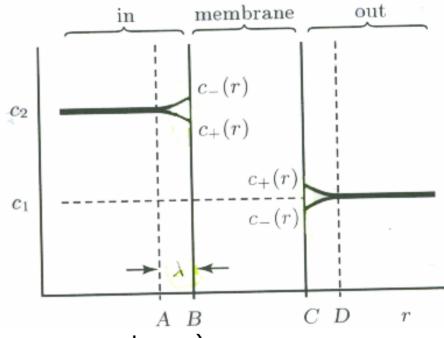
concentration

2.1 Information transmission in neurons

The Nernst Potential:

Example system for **stationary case** (no net flux):

- 2 chambers filled with neutral ion solution: $C_1^+ = C_2^ C_2^+ = C_2^-$
- membrane is only permeable for positive Ions



➔ Positive ions cross the membrane (increase entropy)

 \rightarrow electrical field across the membrane

→ equilibrium

Quantitative description via Boltzmann distribution:

$$\frac{c_2}{c_1} = e^{-\frac{Z \cdot e \cdot \Delta V}{k_B \cdot T}} \implies V_{Nernst} = -\frac{k_B \cdot T}{Z \cdot e} \cdot \ln\left(\frac{c_2}{c_1}\right)$$

(Nernst Potential)



Generalization to more mobile species: The Donnan Potential

Applicable to neuron cell:

- Proteins, DNA, ... (inside): negatively charge and immobilized
- Ions (mainly: K⁺, Na⁺, Cl⁻) diffuse through membrane

Results:

$$V_{\text{mem}} \approx -60 \text{mV} \qquad \text{and} \qquad \frac{c_{Na^+}^{\text{inside}}}{c_{Na^+}^{\text{outside}}} = \frac{c_{K^+}^{\text{inside}}}{c_{K^+}^{\text{outside}}} = \frac{c_{Cl^-}^{\text{outside}}}{c_{Cl^-}^{\text{inside}}}$$

But: Experimentally measured ion-concentration

Ion	Valence z	Interior $c_{2,i}$	Relation	Exterior $c_{1,i}$	Nernst potential $\mathcal{V}_i^{\scriptscriptstyle \mathrm{Nernst}}$
		(тм)		(тм)	(mV)
K ⁺	+1	400	>	20	-75
Na^+	+1	50	<	440	+55
Cl-	-1	52	<	560	-60



So what's wrong?

If you are able to apply equilibrium statistical mechanics to a biological system,

Your system will be dead!

(Pincus Conjecture)

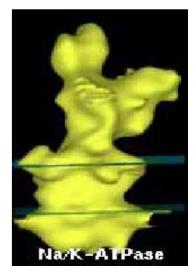
Cells at rest burn food

→ combat the drive towards equilibrium.

In the case of neurons:

Membrane protein Na⁺-K⁺-ATPases pumps:

- Na⁺ to the outside (3 ions per cycle)
- K⁺ to the inside (2 ions per cycle)
- under consumption of ATP





Non-Equilibrium model of membrane-potential:

Ohm's hypothesis:
$$j_i = -g_i \cdot (\Delta V - V_i^{Nernst}) + j_i^{pum_i}$$

(with i=Na⁺,K⁺,...)

with: - ΔV is the membrane potential (charged capacitor)

- generalization of Nernst Potential (non-equilibrium): "translation" of entropic forces into an electrical potential $V^{Nernst} := -\frac{k_B \cdot T}{Z \cdot e} \cdot \ln\left(\frac{c^{in}}{c^{out}}\right)$

- j_i and j_i^{Pump} are current densities

Assumption: steady state:
$$j_i = 0$$
 (more general $\sum_i j_i = 0$)
 $\Rightarrow \underbrace{j_K^{pump} = g_K \cdot (\Delta V - V_K^{Nernst})}_{j_K = 0} = \underbrace{-\frac{2}{3} \cdot j_{Na}^{pump}}_{j_{Na} = 0} = \underbrace{-\frac{2}{3} \cdot g_{Na} \cdot (\Delta V - V_{Na}^{Nernst})}_{j_{Na} = 0}$

with $j_{K}^{pump} = -\frac{2}{3} \cdot j_{Na}^{pump}$ due to the characteristics of the Na-K-ATPase



2.1 Information transmission in neurons

➔ simplified Goldmann-Equation:

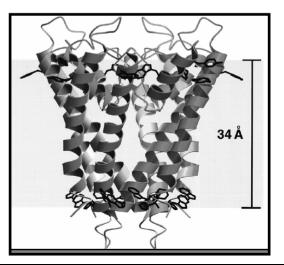
$$\Delta V = \frac{2 \cdot g_{Na} \cdot V_{Na}^{Nernst} + 3 \cdot g_K \cdot V_K^{Nernst}}{2 \cdot g_{Na} + 3 \cdot g_K}$$

Interpretation:

- cell at rest (depolarization): $g_K >> g_{Na}$
 - → membrane potential is dominated by Nernst Potential: $V_{\kappa^{Nernst}} \approx -75 \text{mV}$
- excited cell (action potential): $g_{Na} >> g_{K}$
 - → membrane potential is dominated by Nernst Potential: $V_{Na}^{Nernst} \approx +55 \text{mV}$

Voltage-gated ion channels

- pores in the membrane
- open when the membrane potential exceeds a threshold
- high, ion-specific conductance (when open)





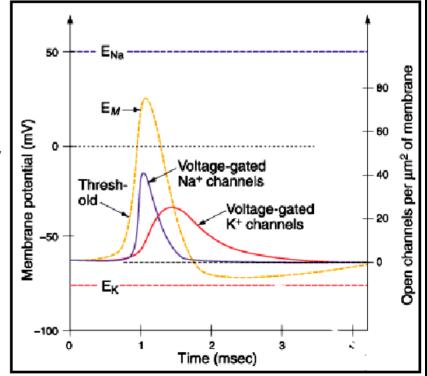
How is an action potential (=nerve impulse) created?

Cell at rest: Na+- and K+-ion-channels closed

→ membrane at rest potential (\approx -65mV)

Excitation above threshold:

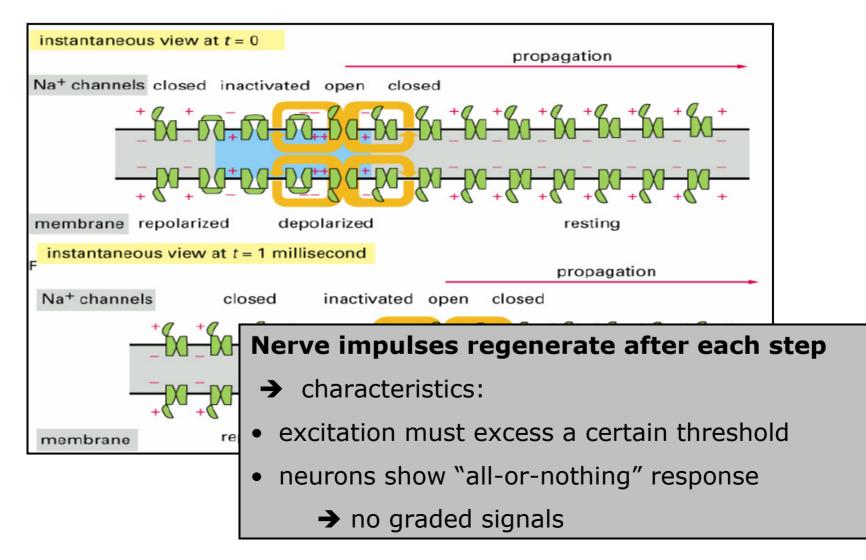
- 1. Na+-channels open
 - → m.p. increases
- K⁺-channels open delayed
 Na-channels close with further delay
 - → m. p. has maximum (\approx +20mV)
 - → cell hyperpolarizes (≈-70mV)
- 3. K+-channels close
 - ➔ membrane at rest potential
- = action potential (AP)





2.1 Information transmission in neurons

Propagation of neuronal signals





2.1 Information transmission in neurons

Summary:

Biological Question:

How can a leaky cable carry a sharp signal over a long distance

Physical answer:

Nonlinearity in a cell membrane's conductance (=*ion channels*) turns the membrane into an excitable medium, which can transmit waves by continuously regenerating (=*action potentials*) them.

➔ Characteristics of information transmission:

- excitation must excess a certain threshold
- neurons show "all-or-nothing" response

 \rightarrow no graded signals

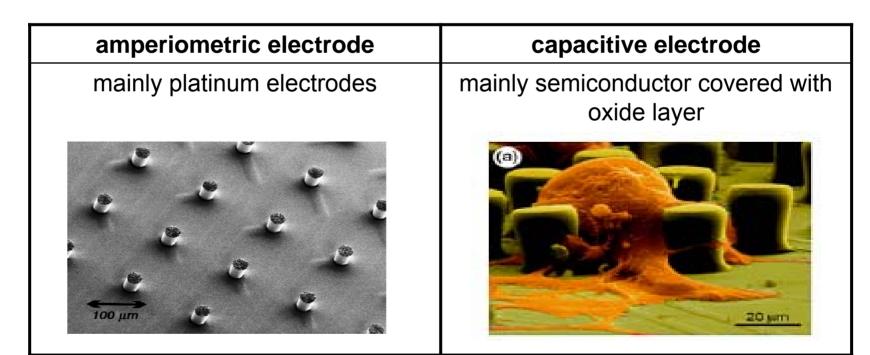


2.2 Electrical stimulation of neuronal activity

2.2 How to stimulate an action potential with a battery?

Answer: Just increase the membrane potential above the threshold with an electrode!

Methods pursued:

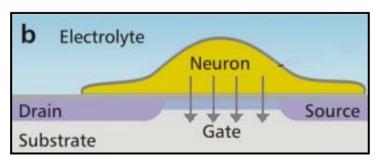




2.2 Electrical stimulation of neuronal activity

The interface:

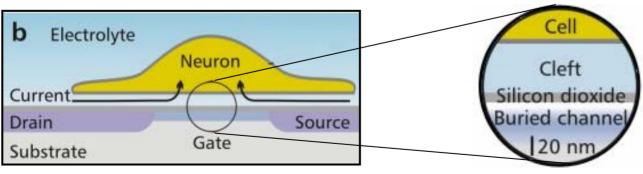
• simplest guess: neuron and substrate form *compact dielectric*



higher charge density in the substrate
→ electric field across the oxide-layer and cell-membrane

= charging a capacitor

real case: conductive cleft between neuron and substrate



higher charge-density in substrate

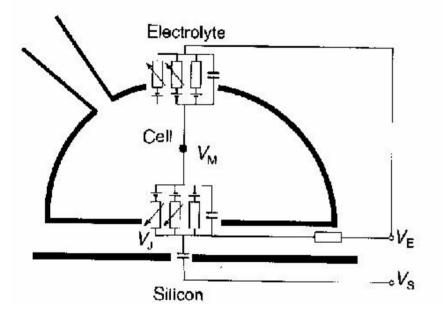
→ current through the conductive cleft ($R \approx M\Omega$) → voltage drop

= Transductive Extracellular Potential



2.2 Electrical stimulation of neuronal activity

Mathematical description:



The planar core-coat-model

Identification of structural elements with parts of electrical circuit, e.g.:

- conductive cleft = resistor
- oxide-layer = capacitor
- membrane = complicated circuit

→ Equivalent circuit

Underlying physical principal:

Kirchhoff's Law

At any point in an electrical circuit the sum of currents flowing towards that point is equal to the sum of currents flowing away from that point.

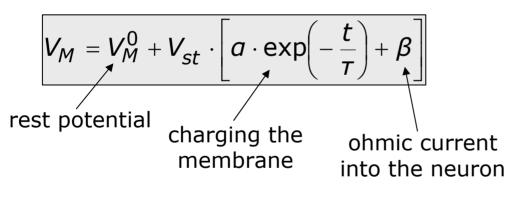
e.g.:
$$\sum_{i} g_{JM}^{i} \left(V_{M} - V_{J} - V_{0}^{i} \right) + c_{M} \left(\frac{dV_{M}}{dt} - \frac{dV_{J}}{dt} \right) = g_{J} \cdot \left(V_{J} - V_{E} \right) + c_{S} \left(\frac{dV_{J}}{dt} - \frac{dV_{S}}{dt} \right)$$



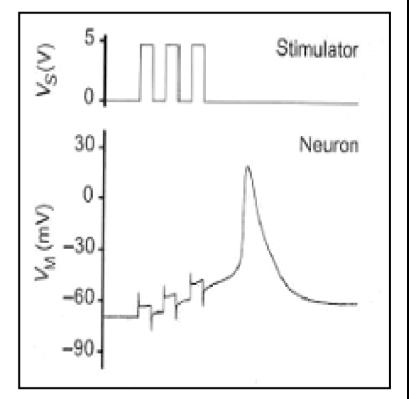
2.2 Electrical stimulation of neuronal activity

Results:

- it is possible to stimulate an action potential electrically
- but: high voltages are needed (\approx 1-5V)



• periodic pulses are most effective

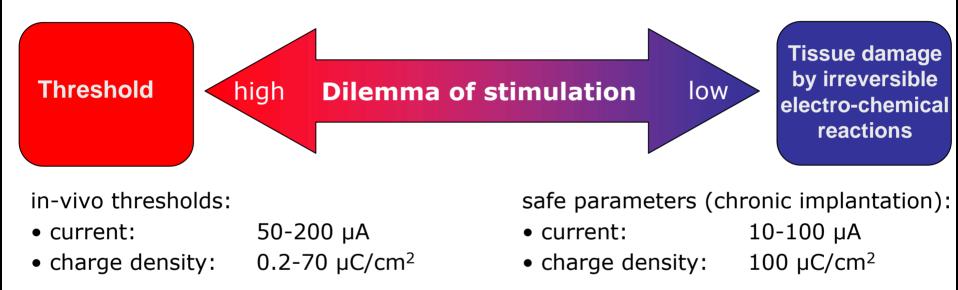


- distance neuron-substrate (cleft thickness) is crucial parameter
 - → surface modification to decrease distance (=nanotechnology)
 e.g. Poly-L-Lysin coating



2.3 Stimulation parameters and electrode design

2.3 Stimulation parameters – a thin line between life and death



But: cochlear implants have helped deafs for years

Other important parameters:

- pulse length
- rate of stimulation
- polarity (anodic/cathodic/bipolar current) \rightarrow wave-form

(a) surface mounted electrode

(b) simple recessed electrode

(c) exponentially recessed electrode

(d) conically recessed electrode

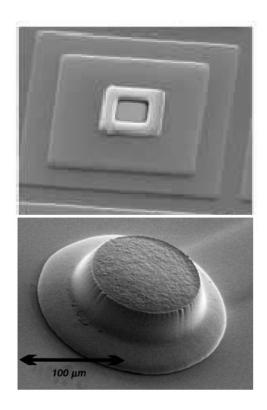
(e) stepwise sampling of a conically recessed electrode



2.3 Stimulation parameters and electrode design

Electrode design:

- high current densities
 - → destruction of tissue by irreversible electrochemical reaction
- delocalized stimulation
 - → low contrast of the perceived picture
- ➔ homogeneous, but localized currents



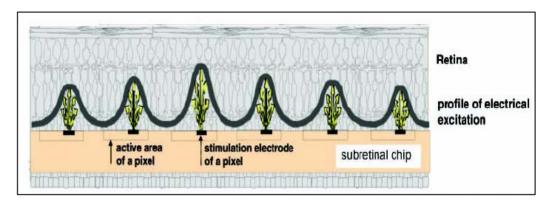


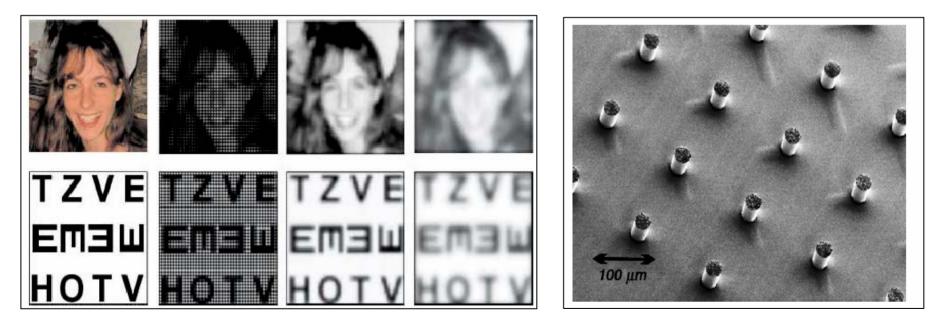
2.3 Stimulation parameters and electrode design

Predicted perception:

Not only a single neuron is stimulated:

- no color-vision
- low contrast vs. pixeled





→ Proper array layout: Distance of electrodes ≈ 70-200 µm

3. How to build an electrical photo sensors?



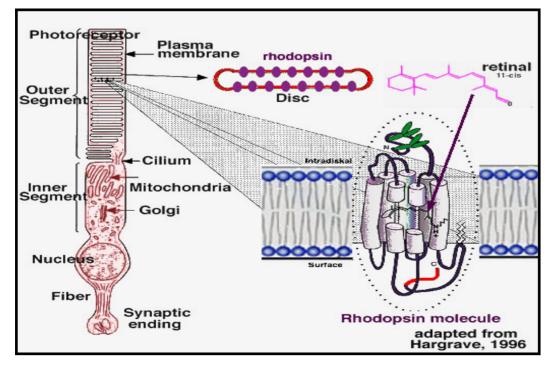
3. Electrical photo sensors

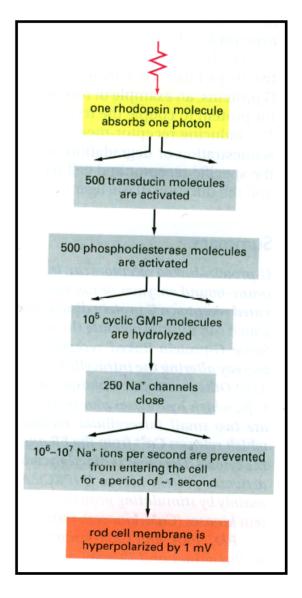
How does the eye sense light?

Rods and Cones contain rhodopsin as photosensitive molecule:

Photon \rightarrow conformational change in chromophore

➔ activation of transduction cascade







3. Electrical photo sensors

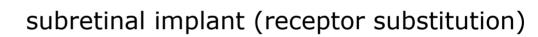
Underlying physical principal:

Photon

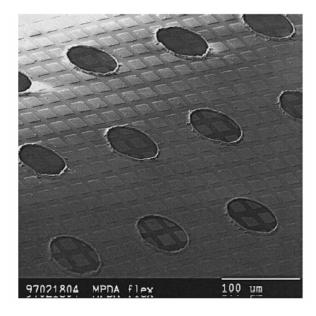
 \rightarrow electric pulse

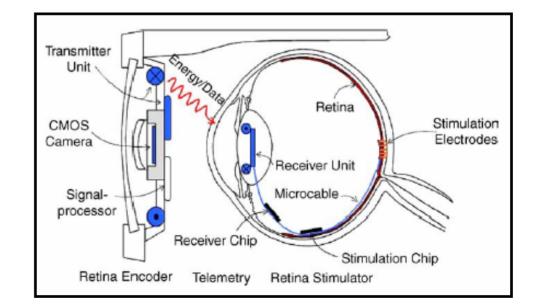
Technical realization:

- solar cell / photodiode \rightarrow
- CCD / CMOS-Camera -



 \rightarrow epiretinal implant (extern camera)



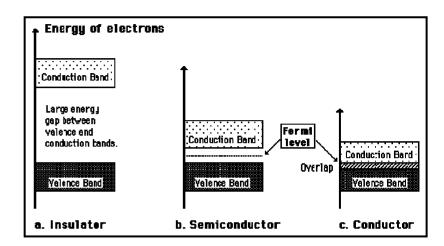


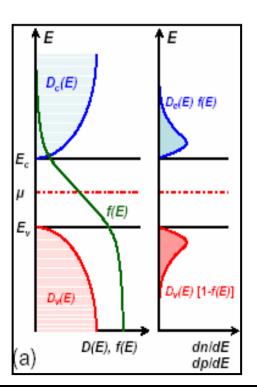


3. Electrical photo sensors

Devices based on semiconductors

→ How do semiconductors work? (a semi-quantitative description)





Intrinsic semiconductors:

Thermal excitation produces electron-hole-pairs, i.e. an electron from the valence band is lifted into the conduction band and leaver a hole charge-carrier densities: $n_c = \frac{1}{V} \cdot \int_{E_c}^{\infty} D_c(E) \cdot f(E,T) dE$ $p_V = \frac{1}{V} \cdot \int_{-\infty}^{E_V} D_V(E) \cdot [1 - f(E,T)] dE$ with $n_c = p_v \implies \mu = E_v + \frac{1}{2} \cdot E_g$ (chem. potential)



3. Electrical photo sensors

Doped semiconductor:

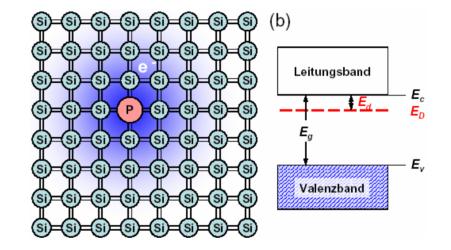
intentional introduction of impurities into a pure semiconductor

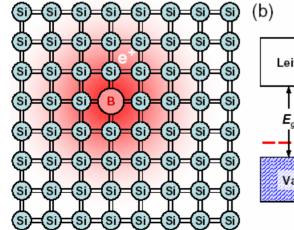
➔ movement of Fermi-level

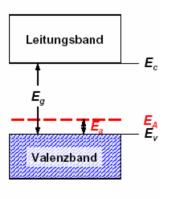
n-type:

introduction of foreign atom with more valence electrons (e.g. P in Si)

➔ more electrons in conduction band







p-type:

introduction of foreign atom with less E_c valence electrons (e.g. B in Si)

➔ more holes in valence band



3. Electrical photo sensors

Inhomogeneous semiconductors: p-n-Interface

One semiconductor is treated with different impurities

e.g. left: p-type right: n-type

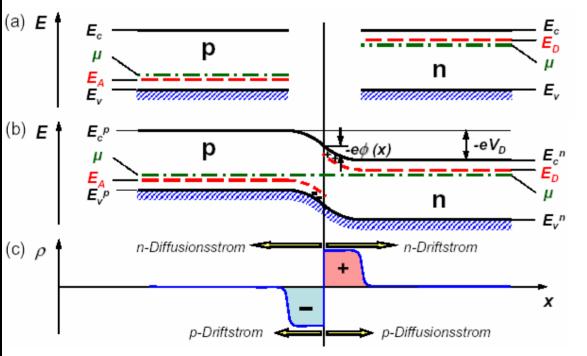
$$N_A(x) = \begin{cases} N_A & \text{für } x < 0 \\ 0 & \text{für } x > 0 \end{cases}$$
$$N_D(x) = \begin{cases} 0 & \text{für } x < 0 \\ N_D & \text{für } x > 0 \end{cases}$$

Separate:

different Fermi-levels

Contact + thermal equilibrium

- \rightarrow same chemical potential
- \rightarrow binding of bands due to depletion layer

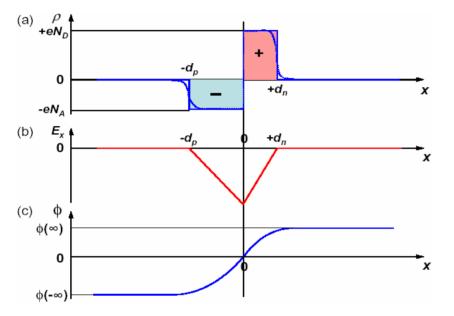




3. Electrical photo sensors

Shottky model:

Depletion layer is homogeneous and sharply bounded

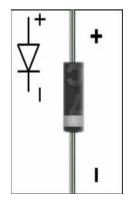


simplified charge distribution

- ➔ linear increase in electric field density
- \rightarrow sigmoidal increase in potential

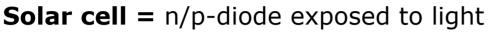
Functionality as diode

- Forward bias: charge carriers move in the "proper" direction of the internal electric field
 - ➔ diode conducts
- Reverse bias: charge carriers move in the "wrong" direction
 - ➔ diode blocks (small reverse current)



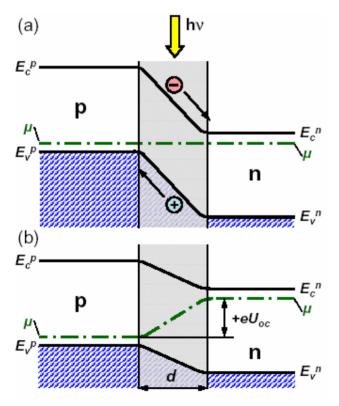


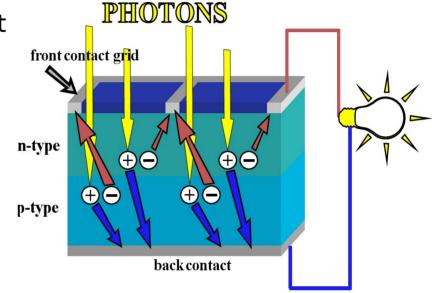
3. Electrical photo sensors



Photons create electron-hole-pairs in the depletion layer

→ charge separation in the internal electric field





- Continuous light-exposure
 - ➔ non-equilibrium:
 - drift-current > diffusive current
 - ➔ Fermi-Level is shifted
 - ➔ potential difference U_{oc} between nand p-type layer



3. Electrical photo sensors

Photodiode

= resistor with resistance that depends on the incoming light intensity

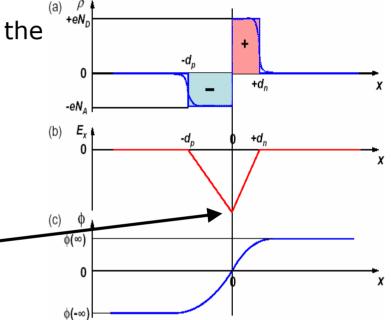
Realization:

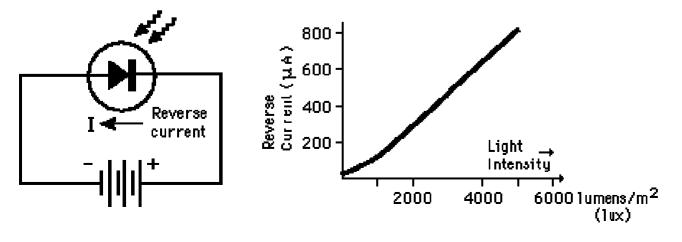
Solar cell run in reverse bias mode

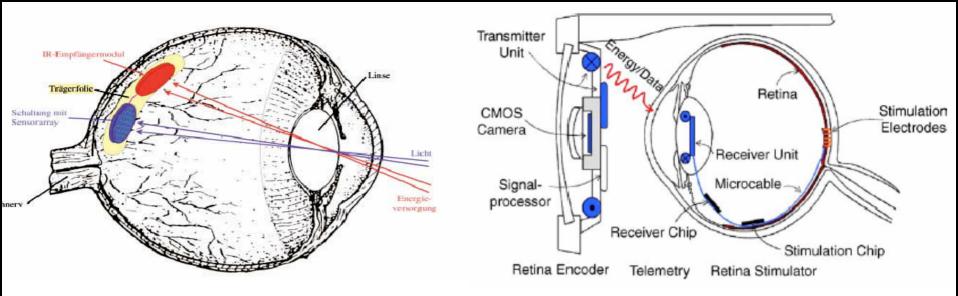
Functionality:

dark: diode blocked ($R \rightarrow \infty$) bright: internal electrical field decreased

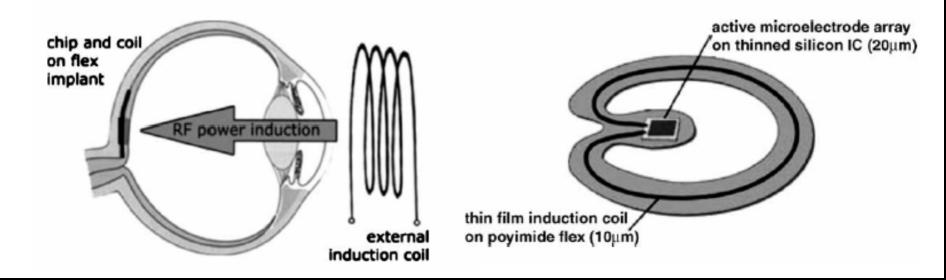
➔ reverse current increases







4. How to supply the implant with power?





4. Power supply and information transmission

Power needed:

- Epiretinal implants (computation +3500 electrodes): \approx 50mW
- Subretinal implants (stimulation): $\approx 200 \text{mW/cm}^2$

Power density in visible light (on retina):

artificial light: ≈ 1mW/cm²
 sunlight (at noon): ≈ 10mW/cm²

Tolerated light intensity of human eye: << 200mW/cm²

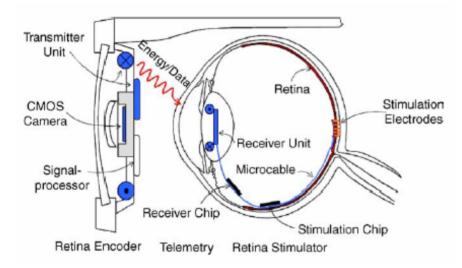
→ Need for wireless power supply!



4. Power supply and information transmission

Solutions:

i) Inductive coupling (for epiretinal implants)



technical properties:

- primary coil: 5cm diameter secondary coil: 1.5mm diameter
- frequency: 1 MHz
- alignment: coplanar (glasses)
 - → efficiency of 2%

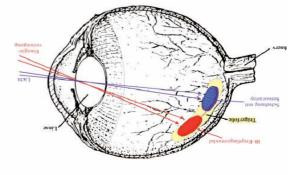
ii) Near-infrared solar-cell (for subretinal implants)

technical properties:

- tolerated NIR power density: \geq 200mW/cm²

LED

- absorption of eye (900nm): \approx 5-10%
- Light generation:



5. Which materials will survive decades of implantation?



5. Suitable materials and encapsulation

Major problems:

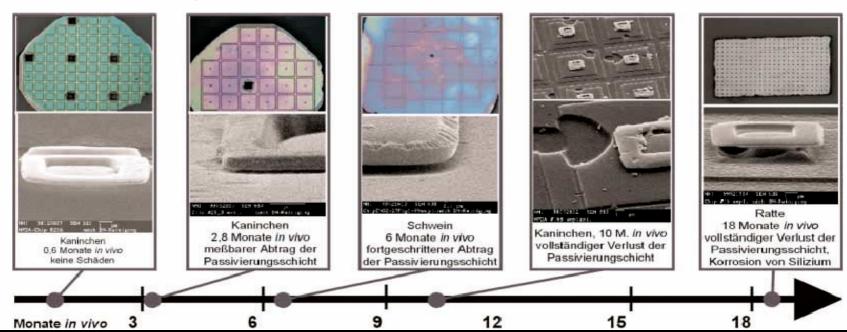
- Biocompatibility:
 - limits for electrical current- and charge-densities
 - avoid infections and inflammation
 - heat drainage
 - surface-functionalization

cochlea implants show longtime acceptance

• Circuit protection

- proper electrode materials:
 - e.g. Pt and alloys with Ir
- encapsulation:
 - e.g. silicon-to-glass solder bonding \rightarrow 10-MPascal-seal

"mild" climate in the eye



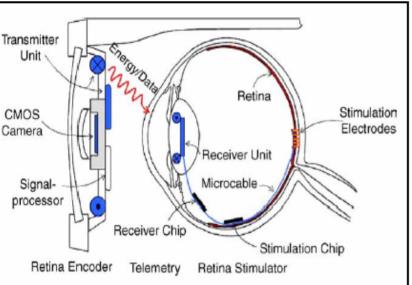
6. State of the art

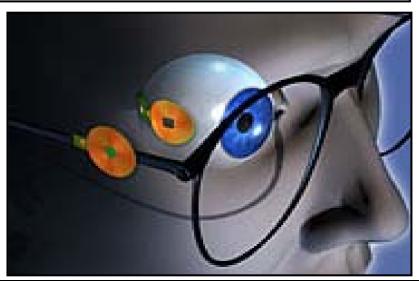
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6. State of the art systems





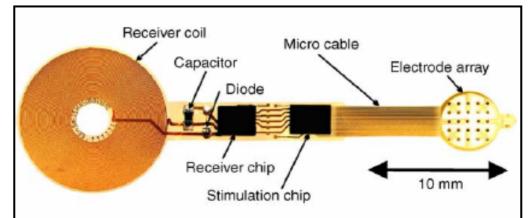
Epiretinal implants:

• Prof. Görtz et al. (Bonn):

- successful test (cortically evoked potentials) in cats and minipigs
- implantation in human patients planed (adaptive patterns generator) after further material test and pattern studies

• Prof. Rizzo et al. (Harvard):

- in-vitro: threshold and stimul. patterns
- in-vivo: study with 6 patients:
 - \rightarrow perception of small light patterns





6. State of the art systems

Subretinal Systems:

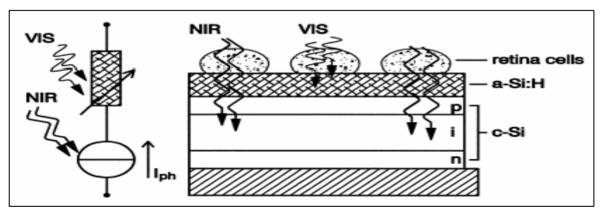
- Prof. Zrenner et al. (Tübingen):
 - Thin film micro photodiode array (MPDA)
 - NIR-cell (doped c-Si): provide voltage 2-3V
 - VIS-photodiode (a-Si:H)

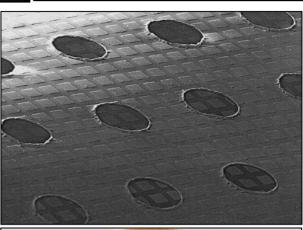
➔ preparations of first study (8 patients)

• Prof. Chow et al. (Chicago):

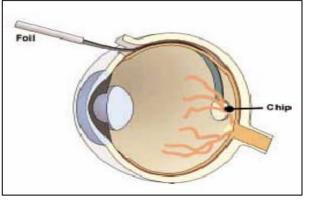
first study with 6 patients over 18 months

- full functionality of electronics after 18mths
- \circ no rejections, infections,...
- visual function improvements: perception of shades of objects but no letters











Sources:

Homepages:

http://www.eye-chip.com (Zrenner et al. / Tübingen)

http://www.pat.rwth-aachen.de (Görtz et al. / Bonn)

http://www.bostonretinalimplant.org/ (Rizzo et al. / Harvard)

http://www.optobionics.com/ (Chow et al. / Chicago)

Publications:

M.B. Schubert et al., Sensors and Actuators (1999): Optimizing photodiode arrays for the use as retinal implants

- M. Görtz et al., Sensors and Actuators (2005): Production processes for a flexible retina implant
- J. Rizzo et al., J. Wyatt et al., American Scientific (2004): Artificial Retina
- A.Y. Chow et al., Arch Ophthalmol (2004) The Artificial Silicon Retina Microchip for the Treatment of Vision Loss From Retinitis Pigm.
- M.S. Humayun et al., J.D. Weinland et al., Survey of Ophthalmology (2002) Retinal Prosthesis for the Blind
- Script of Prof. Gross (TU Munich): Solid State Physic